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In the Claims

- 1. (Currently Amended) A CT detector comprising:
- a scintillator array having a plurality of scintillators; and
- a reflector interstitially disposed between at least two adjacent scintillators, the reflector including a light absorption element disposed between a pair of reflective elements; and
- a reflective layer coated to a face of the scintillator array.
 - (Canceled)
- 3. (Original) The CT detector of claim 1 wherein the light absorption element is configured to reduce optical cross-talk between the at least two adjacent scintillators.
- 4. (Original) The CT detector of claim 3 wherein the light absorption element is configured to substantially eliminate optical cross-talk between the at least two adjacent scintillators.
 - 5. (Canceled)
 - 6. (Canceled)
 - 7. (Canceled)
 - 8. (Canceled)
 - 9. (Canceled)

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- 10. (Canceled)
- 11. (Canceled)
- 12. (Canceled)
- 13. (Original) The CT detector of claim 1 incorporated into a CT imaging system.
- 14. (Original) The CT detector of claim 13 wherein the CT imaging system is configured to acquire radiographic data of a medical patient.
 - 15. (Currently Amended) A CT system comprising:
- a rotatable gantry having a bore centrally disposed therein;
- a table movable fore and aft through the bore and configured to position a subject for C'l' data acquisition;
- a high frequency electromagnetic energy projection source positioned within the rotatable gantry and configured to project high frequency electromagnetic energy toward the subject; and
- and configured to detect high frequency electromagnetic energy projected by the projection source and impinged by the subject, the detector array including:
 - a scintillator array configured to illuminate upon reception of radiographic energy;
 - a reflector assembly disposed between adjacent scintillators of the scintillator array; and

wherein each reflector assembly includes a layer sandwiched between at least a pair of reflective layers; and

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wherein the composite layer includes a high-Z metal and a low-viscosity polymer.

16. (Canceled)

- 17. (Currently Amended) The CT system of claim 16-15 wherein the high Z-metal includes one of tungsten and tantalum.
- 18. (Currently Amended) The CT system of claim $\frac{16}{15}$ wherein the low-viscosity polymer has a non-translucent color.
- 19. (Original) The CT system of claim 15 wherein the at least a pair of reflective layers includes TiO_2 .
- 20. (Original) The CT system of claim 15 wherein each reflective layer has a lateral thickness of approximately 15-90 μm and the composite layer has a lateral thickness of approximately 50-100 μm .
- 21. (Original) The CT system of claim 15 wherein the reflector assembly is cast between adjacent scintillators.
- 22. (Currently Amended) A method of CT detector manufacturing comprising the steps of:

providing a scintillator array of a plurality of scintillators, wherein the step of providing a scintillator array includes the step of forming a substrate of scintillation material;

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disposing a reflective layer between adjacent scintillators; and

disposing a composite layer in the reflective layer.

23. (Canceled)

- 24. (Currently Amended) The method of claim 23 22 further comprising the step of pixelating the substrate.
- 25. (Currently Amended) The method of claim 24 wherein the step of pixelating includes at least one of chemically and mechanically forming gaps in the substrate to define <u>a the</u> plurality of scintillators.
- 26. (Original) The method of claim 25 wherein mechanically forming gaps includes dicing the substrate.
- 27. (Original) The method of claim 25 further comprising the step of depositing reflective material into at least the gaps.
- 28. (Original) The method of claim 27 wherein the step of depositing includes the step of casting.
- 29. (Original) The method of claim 27 wherein the step of disposing a composite layer in the reflective layer includes the step of creating channels in the reflective material.

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- 30. (Original) The method of claim 29 wherein the step of creating includes at least one of laser cutting, wire cutting, and etching.
- 31. (Original) The method of claim 29 further comprising the step of depositing composite material into the channels.
- 32. (Original) The method of claim 31 wherein the composite material includes a metal and a polymer.
- 33. (Original) The method of claim 31 wherein the step of depositing composite material into the channels includes casting.
 - 34. (New) A CT detector comprising:
- a scintillator array having a plurality of scintillators; and
- a reflector interstitially disposed between at least two adjacent scintillators, the reflector including a light absorption element disposed between a pair of reflective elements, wherein the light absorption element is configured to absorb x-rays.
- 35. (New) The CT detector of claim 34 wherein the light absorption element is further configured to absorb approximately 50% of the x-ray photons across a gap between the at least two adjacent scintillators.
 - 36. (New) A CT detector comprising:
- a scintillator array having a plurality of scintillators; and

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a reflector interstitially disposed between at least two adjacent scintillators, the reflector including a light absorption element disposed between a pair of reflective elements, wherein the light absorption element is configured to reduce x-ray punch through.

37. (New) A CT detector comprising:

- a scintillator array having a plurality of scintillators; and
- a reflector interstitially disposed between at least two adjacent scintillators, the reflector including a light absorption element disposed between a pair of reflective elements, wherein the light absorption element includes a high atomic number metal composite.
- 38. (New) The CT detector of claim 37 wherein the metal composite includes a cured metal powder and low viscosity polymer combination.
- 39. (New) The CT detector of claim 38 wherein the polymer includes polyurethane.
- 40. (New) The CT detector of claim 37 wherein the metal composite includes at least one of tungsten, tantalum, and a metal powder with density greater than 16g/cm³.

41. (New) A CT detector comprising:

- a scintillator array having a plurality of scintillators; and
- a reflector interstitially disposed between at least two adjacent scintillators, the reflector including a light absorption element disposed between a pair of reflective elements, wherein the pair of reflective elements include TiO₂.

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42. (New) A CT system comprising:

- a rotatable gantry having a bore centrally disposed therein;
- a table movable fore and aft through the bore and configured to position a subject for CT data acquisition;
- a high frequency electromagnetic energy projection source positioned within the rotatable gantry and configured to project high frequency electromagnetic energy toward the subject; and
- a detector array disposed within the rotatable gantry and configured to detect high frequency electromagnetic energy projected by the projection source and impinged by the subject, the detector array including:
 - a scintillator array configured to illuminate upon reception of radiographic energy;
 - a reflector assembly disposed between adjacent scintillators of the scintillator array; and

wherein each reflector assembly includes a layer sandwiched between at least a pair of reflective layers; and

wherein the at least a pair of reflective layers includes ${\rm TiO}_2$.

43. (New) A CT system comprising:

- a rotatable gantry having a bore centrally disposed therein;
- a table movable fore and aft through the bore and configured to position a subject for CT data acquisition;
- a high frequency electromagnetic energy projection source positioned within the rotatable gantry and configured to project high frequency electromagnetic energy toward the subject; and

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a detector array disposed within the rotatable gantry and configured to detect high frequency electromagnetic energy projected by the projection source and impinged by the subject, the detector array including:

a scintillator array configured to illuminate upon reception of radiographic energy;

a reflector assembly disposed between adjacent scintillators of the scintillator array; and

wherein each reflector assembly includes a layer sandwiched between at least a pair of reflective layers; and

wherein each reflective layer has a lateral thickness of approximately 15-90 μm and the composite layer has a lateral thickness of approximately 50-100 μm .

44. (New) A CT system comprising:

- a rotatable gantry having a bore centrally disposed therein;
- a table movable fore and aft through the bore and configured to position a subject for CT data acquisition;
- a high frequency electromagnetic energy projection source positioned within the rotatable gantry and configured to project high frequency electromagnetic energy toward the subject; and
- a detector array disposed within the rotatable gantry and configured to detect high frequency electromagnetic energy projected by the projection source and impinged by the subject, the detector array including:
 - a scintillator array configured to illuminate upon reception of radiographic energy;
 - a reflector assembly disposed between adjacent scintillators of the scintillator array; and

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wherein each reflector assembly includes a layer sandwiched between at least a pair of reflective layers; and wherein the reflector assembly is cast between adjacent scintillators.